

Photoacoustic wavefront shaping to focus light in deep tissue: a computational feasibility study

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We use computational methods to investigate the requirements

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 - 4. Simulating the propagation of light through tissue-like media

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 - 7. Investigate the sensitivity requirements of a PAWS system

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- 3. Conclusions
- 4. Acknowledgements

Consider trying to focus light inside biological tissue:



Horstmeyer, R., et al., Nature Photonics, 2015

Consider trying to focus light inside biological tissue: A modulation is needed to shape light.

Horstmeyer, R., et al., Nature Photonics, 2015

Consider trying to focus light inside biological tissue: A modulation is needed to shape light. When focusing through a medium, speckle can be enlarged and used directly for feedback to shape incident light.

Horstmeyer, R., et al., Nature Photonics, 2015



Horstmeyer, R., et al., Nature Photonics, 2015



Chaigne et al., Nature Photonics 2015



Chaigne et al., Nature Photonics 2015



Challenges with PAWS

Number of input modes

- Size of target defined by acoustic diffraction limit.
- Volume encompasses many optical speckle.
- Large number of input modes needed







Challenges with PAWS

light, e.g. SLM elements Volume encompasses

- many optical speckle.
- Large number of input modes needed









Challenges with PAWS

Number of input modes

- Size of target defined by acoustic diffraction limit.
- Volume encompasses many optical speckle.
- Large number of input modes needed

• Mode is we into r

Sensitivity of PAWS system

- Modulation per input mode is weaker when focusing into multiple speckle.
- High sensitivity required to detect this modulation



Chaigne et al., Nature Photonics 2015



Chaigne et al., Nature Photonics 2015

















Our method for simulating WFS

- 1. Design domain with Mie theory
- 2. Simulate the propagation of plane wave at different angles [input modes].





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- Optimize phase of each plane wave 3.





Using iterative phase modulation to focus through TiO₂ (can we model WFS?)



Vellekoop and Mosk, Optics letters, 2007

Replicate Vellekoop & Mosk

 $10\mu m TiO_2$ phantom with transport mean free path of ~ $5\mu m^{-1}$).

441 input modes





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Simulating the propagation light through tissue-like media



Simulating the propagation light through tissue-like media



Validating tissue-like domains and the T-matrix method

- Numerical validation through comparison with Mie theory & Finite-Difference Time-Domain [are the simulated fields correct?]
- **Domain validation** with Monte Carlo and Inverse Adding doubling. [is the domain large enough?]













Avefront shaping challenging?





- PAWS cannot focus light into a single speckle
- Constrained by acoustic diffraction limit.
- Many more input modes required.



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Number of modes required to generate foci with a given enhancement grows rapidly.





Consider focusing into a single speckle vs multiple speckles: $\int_{a}^{b} \int_{a}^{b} \int$

- 1. More input modes are required to achieve a focus with a given intensity.
- 2. Not every speckle can be made to constructively interfere simultaneously:
 - For fully developed speckle some grains will always be out of phase and destructively interfere.
 - The enhancement per modulation approaches zero as the number of speckle increases.

Consider focusing into a single speckle vs multiple speckles:



2. Not every speckle can be made to constructively interfere simultaneously:

x [µm]

 For fully developed speckle some grains will always be out of phase and destructively interfere.

x [µm]

• The enhancement per modulation approaches zero as the number of speckle increases.

Increased sensitivity requirements of a PAWS system to detect the effect of a given modulation

0.9

frequency 9.0 9.0

Normalized f 0.2 0.3 0.3

0.1

-1.5



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Increased sensitivity requirements of a PAWS system to detect the effect of a given modulation







100 Can be used to measure amplitude and phase of light shaped into 20 any desired field.

Measuring the angular memory effect range

Ansatz methods have struggled to model y [µm] coherent phenomena (e.g. memory correlations) Some methods exploit these correlations to focus light into scattering media.



Focusing into arbitrary fields 10 80 [µm] 60 > 40 -5 -10 -5 0 5 10 -10 x [µm]



Measuring the angular memory effect range

Ansatz methods have struggled to model y [µm] coherent phenomena (e.g. memory correlations) Some methods exploit these correlations to focus light into scattering media.





Modelling the angular range of an optimized focus

Imaging FOV could be increased by exploiting memory correlations to translate already optimized foci.

Focusing might also be able to be accelerated by exploiting priors (e.g. sharing phase maps between input modes).



Conclusions

15

10

5

0

-5

-10

-15

-60

x [μm]

- 1. PAWS has the potential to enhance the depth of optical imaging modalities.
- 2. **Rigorous computational model can be used to** investigate the challenges of achieving an internal focusing using PAWS.
- 3. Our proposed model can be used to investigate the requirements of a PAWS system, and how correlations inside biological tissue can be exploited.

I'm happy to chat about any of my research, and if you're particularly interested in the model please review my talk yesterday (12388-15).

-40



Input modes = 1

|E|

Acknowledgements

Email: jake.bewick.18@ucl.ac.uk

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National Institute for Health Research



Contact details



UCL





Simulating the propagation light through tissue-like media

